



Hyers-Ulam Stability and Control of Fractional Glucose-Insulin Systems

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Abstract. This paper presents a novel fractional-order model for glucose-insulin dynamics using the Caputo-Fabrizio (CF) derivative, which accounts for memory effects through its nonsingular exponential kernel. Existence and uniqueness of the solution are established via fixed point theory, and infinite series solutions are obtained using the Sumudu transform. Hyers-Ulam stability is analyzed to assess the system's robustness against perturbations. A linear control strategy is introduced to regulate glucose levels, demonstrating potential for integration with real-time insulin delivery systems. Compared to classical integer-order models, the proposed approach provides improved accuracy, enhanced stability, and deeper insight into the chaotic behavior of glucose-insulin interactions. This framework supports the development of personalized diabetes treatment and adaptive control strategies.

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1. Introduction

The prevalence of diabetes among adults worldwide has increased to over 422 million, according to WHO [1]. Diabetes and its complications have been studied extensively over the last decade, highlighting the need for long-term management. Diabetes burden can be reduced through early detection and prevention [2]. A healthcare professional is essential

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in managing a patient's condition and preventing complications [3]. Literature on glucose-insulin dynamics, epidemiology, complications, and the economic burden of diabetes is growing. Many mathematical, statistical, and computational algorithms have been proposed to help us understand diabetes [4, 5]. The studies cover the range of topics discussed above, such as the dynamics of glucose and insulin in relation to insulin [6, 7], computer algorithms and devices [8–10], and the costs associated with diabetes [11, 12]. Additionally, research has been conducted on the psychosocial aspects of diabetes, such as quality of life and social support [13, 14], and its impact on public health [15]. A recent development in fractional calculus has been its ability to model complex systems with arbitrary differentiation orders. Diabetes research has benefited from enhanced modeling of glucose-insulin dynamics, as well as complications associated with diabetes [16, 17]. In addition to the Riemann-Liouville, Caputo, and Caputo-Fabrizio (CF) fractional calculus operators, Atangana-Baleanu can be used to capture power laws and exponential decay [18]. The CF operator, which has a nonsingular kernel, has successfully been applied to glucose-insulin modeling, providing insights into memory effects and chaos within the system [19–54]. Sadek et al. (2024) introduced novel Θ -fractional operators, expanding the framework of fractional calculus and demonstrating their efficiency in optimization problems using the Galerkin-Bell method [55]. In [56], Sadek proposed a cotangent fractional derivative, providing an alternative approach to solving complex differential equations with applications in fractional modeling. In the context of epidemiology, Sadek et al. [57] developed a fractional-order model to predict COVID-19 dynamics in Morocco, incorporating isolation and vaccination strategies, where the inclusion of memory effects improved predictive accuracy [58]. Additionally, Sadek et al. (2022) applied fractional calculus to model the synthesis of TiO_2 nanopowder via the sol-gel method at low temperatures, capturing the complexities of nanopowder formation and improving process modeling in nanotechnology [59]. These contributions collectively enhance the theoretical and applied aspects of fractional calculus, demonstrating its versatility across diverse scientific domains.

An exponential decay function is used to model the fractional differential operator to understand how memory impacts fractional glucose-insulin regulation. With this kernel, we can study memory effects. Using Caputo-Fabrizio fractional operators to analyze fractional variable-order glucose-insulin regulation, memory effects enhance stability and synchronization. It highlights the potential for developing more effective diabetes control strategies based on uniqueness and boundedness. We also examine Caputo-Fabrizio fractional variable-order glucose-insulin regulation, demonstrating that fractional chaotic systems can be synchronized. Fixed point theory is used to prove uniqueness and boundedness of solutions, and CF fractions are used to analyze Hyers-Ulam stability. Sumudu transforms are used to derive infinite series solutions that demonstrate efficiency. Different smooth functions defined in $(0,1]$ can be used to simulate fractional derivatives.

Our novel fractional-order glucose-insulin model incorporates memory effects and non-local interactions based on the Caputo-Fabrizio derivative. Compared to traditional integer-order models, this approach offers a more accurate representation of physiological processes. Using Sumudu transforms for solution derivation enhances computational efficiency and reduces numerical errors. Based on Hyers-Ulam stability analysis, our model

is robust against perturbations, while a newly developed linear control strategy effectively regulates glucose levels, with potential applications in real-time insulin delivery. Based on the results, fractional-order derivatives provide a more accurate and stable representation of glucose-insulin fluctuations. Moreover, our model simulates disease progression, optimizes insulin dosage for personalized treatment, and stabilizes extreme glucose variations, which prevents severe complications such as hypoglycemia and hyperglycemia. In contrast to previous studies, our approach provides novel insights into chaotic dynamics in glucose regulation, which contributes to the efficient management of diabetes.

A key aspect of this paper is the utilization of Caputo-Fabrizio-Caputo fractional derivatives, which possess a non-singular kernel, enabling an accurate description of diverse physiological processes. Diabetes patients can analyze glucose-insulin interactions and gain insight into memory and chaotic behaviors with the CF-based glucose-insulin regulation model. The model can also be used to develop advanced control strategies. The proposed model outperforms glucose-insulin models with integer-order derivatives. Real-world implementation of this model may be challenging due to fractional derivatives and variable orders. Additionally, collecting and analyzing physiological parameters is complex. The model must be validated across diverse patient populations to ensure robustness and reliability.

The CF fractional-order glucose-insulin system requires linear controllers to achieve equilibrium. Diabetes management is significantly improved when blood glucose levels are controlled precisely. Based on real-time glucose monitoring, advanced insulin pumps could automatically adjust insulin delivery. In addition, patients may benefit from personalized treatment plans that optimize insulin dosing. Chaos control and synchronization are influenced by the CF fractional-order framework, where variable orders simulate fractional derivatives. Through variable orders, Caputo-Fabrizio fractional chaotic systems can be synchronized. Furthermore, variable orders allow for fine-tuning fractional derivatives' chaotic behavior. Compared to conventional integer-order derivatives, the proposed model demonstrates superior glucose-insulin regulation performance, showing its potential for real-world application.

2. Glucose-Insulin Model

In 1939, Himsworth and Ker introduced in vivo measurement of insulin sensitivity using experimental methods, which revolutionized the modeling of glucose-insulin dynamics [60]. In various physiological contexts, mathematical models have been developed to estimate glucose disappearance and insulin-glucose dynamics. One of the pioneers in this field was Bolie, who presented a simple mathematical model in 1961 [61]. Model based on ordinary differential equations (ODEs):

$$\begin{aligned}\frac{d\tilde{u}}{dt} &= -b_1\tilde{u} - b_2\tilde{v} + d_1, \\ \frac{d\tilde{v}}{dt} &= -b_3\tilde{u} - b_4\tilde{v},\end{aligned}$$

where $\tilde{u}(t)$ represents the glucose concentration, $\tilde{v}(t)$ represents the insulin concentration, and d_1, b_1, b_2, b_3, b_4 are model parameters.

A well-known minimal model for glucose-insulin dynamics was proposed by Bergman and Cobelli in the mid-1980s, focusing on insulin sensitivity [62]. This model has been instrumental in advancing our understanding of glucose-insulin interactions and can be expressed as follows:

$$\begin{aligned}\frac{d\tilde{u}(t)}{dt} &= -(q_1 + \tilde{w}(t))\tilde{u}(t) + q_1\tilde{u}_b, & \tilde{u}(0) &= \tilde{u}_0, \\ \frac{d\tilde{w}(t)}{dt} &= -q_2\tilde{w}(t) + q_3(\tilde{v}(t) - \tilde{v}_b), & \tilde{w}(0) &= 0, \\ \frac{d\tilde{v}(t)}{dt} &= q_4(\tilde{u}(t) - q_5)^+ - q_6(\tilde{v}(t) - \tilde{v}_b), & \tilde{v}(0) &= \tilde{v}_0 + \tilde{v}_b,\end{aligned}$$

where $\tilde{u}(t)$ is the glucose concentration, $\tilde{w}(t)$ is an auxiliary variable representing the activity of insulin-sensitive tissues, and $\tilde{v}(t)$ is the insulin concentration. The symbol $(\tilde{u}(t) - q_5)^+$ represents the positive part of $\tilde{u}(t) - q_5$, and the parameters q_1, q_2, \dots, q_6 are model-specific constants.

The minimal model has been extensively used to describe glucose tolerance tests (OGTTs) and meal tests [63]. With this method, insulin sensitivity can be estimated without a glucose clamp experiment $S_x = \frac{q_3}{q_2}$. Physical exercise affects glucose-insulin dynamics according to Derouich and Boutayeb [64]. Physical activity is included in their model as follows:

$$\begin{aligned}\frac{d\tilde{u}(t)}{dt} &= -(1 + r_2)\tilde{v}(t)\tilde{u}(t) + (q_1 + r_1)(\tilde{u}_b - \tilde{u}(t)), \\ \frac{d\tilde{v}(t)}{dt} &= -q_2\tilde{v}(t) + (q_3 + r_3)(\tilde{v}(t) - \tilde{v}_b),\end{aligned}$$

where r_1, r_2, r_3 represent parameters related to physical exercise, which accelerates glucose utilization by muscles, increases insulin sensitivity, and improves glucose disposal.

Other models, such as those developed by Gaetano and Arino [65], utilize delay differential equations (DDEs) to capture more complex glucose-insulin interactions. The dynamical delay differential model is given by:

$$\begin{aligned}\frac{d\tilde{u}(t)}{dt} &= -c_1\tilde{u}(t) - c_4\tilde{v}(t)\tilde{u}(t) + c_7, & \tilde{u}(0) &= \tilde{u}_b + c_0, \\ \frac{d\tilde{v}(t)}{dt} &= -c_2\tilde{v}(t) + \frac{c_6}{c_5} \int_{t-c_5}^t G(s)ds, & \tilde{v}(0) &= \tilde{v}_b + c_3c_0,\end{aligned}$$

with $\tilde{u}(t) = \tilde{u}_b$ for $-c_5 \leq t < 0$. There has been an increase in complexity in the field of glucose-insulin modeling as a result of the exploration of fractional-order systems.

In [66], Shabestari et al. proposed a model based on the Lotka-Volterra framework [67], incorporating fractional dynamics to analyze the glucose-insulin relationship. The

fractional model is as follows:

$$\begin{aligned}\dot{u} &= -\mathbf{b}_1\check{u} + \mathbf{b}_2\check{u}\check{v} + \mathbf{b}_3\check{v}^2 + \mathbf{b}_4\check{v}^3 + \mathbf{b}_5\check{w} + \mathbf{b}_6\check{w}^2 + \mathbf{b}_7\check{w}^3 + \mathbf{b}_{20}, \\ \dot{v} &= -\mathbf{b}_8\check{u}\check{v} - \mathbf{b}_9\check{u}^2 - \mathbf{b}_{10}\check{u}^3 + \mathbf{b}_{11}\check{v}(1 - \check{v}) - \mathbf{b}_{12}\check{w} - \mathbf{b}_{13}\check{w}^2 - \mathbf{b}_{14}\check{w}^3 + \mathbf{b}_{21}, \\ \dot{w} &= \mathbf{b}_{15}\check{v} + \mathbf{b}_{16}\check{v}^2 + \mathbf{b}_{17}\check{v}^3 - \mathbf{b}_{18}\check{w} - \mathbf{b}_{19}\check{v}\check{w}.\end{aligned}$$

with the initial conditions: $\check{u}(0) = \check{u}_0$, $\check{v}(0) = \check{v}_0$, $\check{w}(0) = \check{w}_0$. Here: \check{u} represents glucose concentration, \check{v} represents insulin concentration, and \check{w} represents the population density of β -cells. The parameters \mathbf{b}_i for $i = 1, 2, \dots, 21$, describe various interaction rates which can be defined in Table 1.

Glucose-insulin regulatory system expressed as Caputo derivative through fractional calculus:

$$\begin{aligned}{}^C\mathcal{D}_t^{\check{\alpha}(t)}\check{u} &= -d_1\check{u} + d_2\check{u}\check{v} + d_3\check{v}^2 + d_4\check{v}^3 + d_5\check{w} + d_6\check{w}^2 + d_7\check{w}^3 + d_{20}, \\ {}^C\mathcal{D}_t^{\check{\alpha}(t)}\check{v} &= -d_8\check{u}\check{v} - d_9\check{u}^2 - d_{10}\check{u}^3 + d_{11}\check{v}(1 - \check{v}) - d_{12}\check{w} - d_{13}\check{w}^2 - d_{14}\check{w}^3 + d_{21}, \\ {}^C\mathcal{D}_t^{\check{\alpha}(t)}\check{w} &= d_{15}\check{v} + d_{16}\check{v}^2 + d_{17}\check{v}^3 - d_{18}\check{w} - d_{19}\check{v}\check{w},\end{aligned}$$

where all parameter d_i , $i = 1, 2, \dots, 21$ are described in Table 1. CF fractional operators have been applied to model glucose-insulin dynamics, offering new insights into the system's chaotic behavior. Models of this type can be expressed as follows:

$$\begin{aligned}{}^{CF}\mathcal{D}_{0,t}^{\check{\alpha}}\check{u} &= -d_1\check{u} + d_2\check{u}\check{v} + d_3\check{v}^2 + d_4\check{v}^3 + d_5\check{w} + d_6\check{w}^2 + d_7\check{w}^3 + d_{20}, \\ {}^{CF}\mathcal{D}_{0,t}^{\check{\alpha}}\check{v} &= -d_8\check{u}\check{v} - d_9\check{u}^2 - d_{10}\check{u}^3 + d_{11}\check{v}(1 - \check{v}) - d_{12}\check{w} - d_{13}\check{w}^2 - d_{14}\check{w}^3 + d_{21}, \\ {}^{CF}\mathcal{D}_{0,t}^{\check{\alpha}}\check{w} &= d_{15}\check{v} + d_{16}\check{v}^2 + d_{17}\check{v}^3 - d_{18}\check{w} - d_{19}\check{v}\check{w}.\end{aligned}\quad (1)$$

The control fractional order of time-varying glucose-insulin regulation is

$$\begin{aligned}{}^{CF}\mathcal{D}_{0,t}^{\check{\alpha}}\check{u} &= -d_1\check{u} + d_2\check{u}\check{v} + d_3\check{v}^2 + d_4\check{v}^3 + d_5\check{w} + d_6\check{w}^2 + d_7\check{w}^3 + d_{20} - c_1(\check{u} + \check{v}), \\ {}^{CF}\mathcal{D}_{0,t}^{\check{\alpha}}\check{v} &= -d_8\check{u}\check{v} - d_9\check{u}^2 - d_{10}\check{u}^3 + d_{11}\check{v}(1 - \check{v}) - d_{12}\check{w} - d_{13}\check{w}^2 - d_{14}\check{w}^3 + d_{21}, \\ {}^{CF}\mathcal{D}_{0,t}^{\check{\alpha}}\check{w} &= d_{15}\check{v} + d_{16}\check{v}^2 + d_{17}\check{v}^3 - d_{18}\check{w} - d_{19}\check{v}\check{w} - c_2(\check{u} + \check{v}),\end{aligned}\quad (2)$$

where c_1, c_2 are positive constants.

3. Preliminaries

This part of the manuscript introduces essential concepts and preliminary definitions that are crucial for understanding the subsequent sections.

Definition 1 ([68]). Let $\varphi \in \mathcal{H}^1(a, b)$, where $b > a$ and $\check{\alpha} \in (0, 1)$. The CF derivative is defined as follows:

$${}^{CF}\mathcal{D}_t^{\check{\alpha}}\varphi(t) = \frac{\check{N}(\check{\alpha})}{1 - \check{\alpha}} \int_a^t \varphi'(\theta) \exp\left[-\frac{t - \theta}{1 - \theta}\right] d\theta.$$

Here, $\check{N}(\check{\alpha})$ is a normalization function, where $\check{N}(1) = \check{N}(0) = 1$. If φ does not belong to $\mathcal{H}^1(a, b)$, then the CF derivative can be redefined as:

$${}^{CF}\mathcal{D}_t^{\check{\alpha}}\varphi(t) = \frac{\check{N}(\check{\alpha})}{1 - \check{\alpha}} \int_{\alpha}^t [\varphi(t) - \varphi(\theta)] \exp\left[-\frac{t - \theta}{1 - \theta}\right] d\theta.$$

Definition 2 ([69]). Let $\check{\alpha} \in (0, 1]$. The fractional integral of order $\check{\alpha}$ for a function φ is expressed as:

$${}^{CF}I_t^{\check{\alpha}}\varphi(t) = \frac{(1 - \check{\alpha})}{\check{N}(\check{\alpha})}\varphi(t) + \frac{\check{\alpha}}{\check{N}(\check{\alpha})}\varphi(t) \int_0^t \varphi(\theta)d\theta.$$

Definition 3 ([70, 71]). The Laplace transform of the CF derivative $M(t)$ is formulated as:

$$\mathcal{L} [{}^{CF}\mathcal{D}_t^{\check{\alpha}}M(t)] = \frac{s\mathcal{L}[M(t)] - M(0)}{s + \check{\alpha}(1 - s)}, \quad s \geq 0, \quad \check{\alpha} \in (0, 1].$$

The Sumudu transform, often utilized in fractional calculus applications, builds upon integral transform techniques [31, 32]. Let us consider a function space defined as follows:

$$\mathbb{A} = \left\{ \phi : \exists \check{\alpha}, c_1, c_2 \geq 0 \text{ such that } |\phi(t)| < \check{\alpha} \exp\left(\frac{t}{c_j}\right), \quad t \in (-1)^j \times [0, \infty) \right\},$$

and define the Sumudu transform of $\phi(t) \in \mathbb{A}$ by:

$$\text{ST}[\phi(t)](s) = \frac{1}{s} \int_0^{\infty} \exp\left(-\frac{t}{s}\right) \phi(t)dt,$$

where the inverse transform is denoted by $\phi(t) = \text{ST}^{-1}[\phi(s)]$.

The Sumudu transform of the CF derivative is given by [33]:

$$\text{ST} [{}^{CF}\mathcal{D}_0^{\check{\alpha}}\phi(t)](s) = \frac{\check{N}(\check{\alpha})}{1 - \check{\alpha} + \check{\alpha}s} (\text{ST}[\phi(t)](s) - \phi(0)).$$

4. Existence and Uniqueness

In this section, we are going to discuss the existence and uniqueness of the solutions [34] of the Caputo Fabrizio fractional model with initial conditions in system (1). By using Caputo-Fabrizio fractional integral operator on the above system, we get

$$\begin{aligned} \check{u} - \check{u}(0) &= {}^{CF}I_t^{\check{\alpha}} \left[-d_1 \check{u} + d_2 \check{u}\check{v} + d_3 \check{v}^2 + d_4 \check{v}^3 + d_5 \check{w} + d_6 \check{w}^2 + d_7 \check{w}^3 + d_{20} \right], \\ \check{v} - \check{v}(0) &= {}^{CF}I_t^{\check{\alpha}} \left[-d_8 \check{u}\check{v} - d_9 \check{u}^2 - d_{10} \check{u}^3 + d_{11} \check{v}(1 - \check{v}) - d_{12} \check{w} - d_{13} \check{w}^2 - d_{14} \check{w}^3 + d_{21} \right], \\ \check{w} - \check{w}(0) &= {}^{CF}I_t^{\check{\alpha}} \left[d_{15} \check{v} + d_{16} \check{v}^2 + d_{17} \check{v}^3 - d_{18} \check{w} - d_{19} \check{v}\check{w} \right]. \end{aligned}$$

The kernels of the system are:

$$\begin{aligned}\Lambda_1(t, \tilde{u}, \tilde{v}, \tilde{w}) &= -d_1 \tilde{u} + d_2 \tilde{u}\tilde{v} + d_3 \tilde{v}^2 + d_4 \tilde{v}^3 + d_5 \tilde{w} + d_6 \tilde{w}^2 + d_7 \tilde{w}^3 + d_{20}, \\ \Lambda_2(t, \tilde{u}, \tilde{v}, \tilde{w}) &= -d_8 \tilde{u}\tilde{v} - d_9 \tilde{u}^2 - d_{10} \tilde{u}^3 + d_{11} \tilde{v}(1 - \tilde{v}) - d_{12} \tilde{w} - d_{13} \tilde{w}^2 - d_{14} \tilde{w}^3 + d_{21}, \\ \Lambda_3(t, \tilde{u}, \tilde{v}, \tilde{w}) &= d_{15} \tilde{v} + d_{16} \tilde{v}^2 + d_{17} \tilde{v}^3 - d_{18} \tilde{w} - d_{19} \tilde{v}\tilde{w}.\end{aligned}$$

We will assume that \tilde{u}, \tilde{v} and \tilde{w} are nonnegative bounded functions according to previous theorem.

With the Caputo Fabrizio fractional integral to Eq. (1), we have

$$\begin{aligned}\tilde{u} - \tilde{u}(0) &= \frac{2(1-\tilde{\alpha})}{(2-\tilde{\alpha})N(\tilde{\alpha})} \left(\Lambda_1(t, \tilde{u}, \tilde{v}, \tilde{w}) \right) + \frac{2\tilde{\alpha}}{(2-\tilde{\alpha})N(\tilde{\alpha})} \int_0^t \left(\Lambda_1(s, \tilde{u}(s), \tilde{v}(s), \tilde{w}(s)) \right) ds, \\ \tilde{v} - \tilde{v}(0) &= \frac{2(1-\tilde{\alpha})}{(2-\tilde{\alpha})N(\tilde{\alpha})} \left(\Lambda_2(t, \tilde{u}, \tilde{v}, \tilde{w}) \right) + \frac{2\tilde{\alpha}}{(2-\tilde{\alpha})N(\tilde{\alpha})} \int_0^t \left(\Lambda_2(s, \tilde{u}(s), \tilde{v}(s), \tilde{w}(s)) \right) ds, \\ \tilde{w} - \tilde{w}(0) &= \frac{2(1-\tilde{\alpha})}{(2-\tilde{\alpha})N(\tilde{\alpha})} \left(\Lambda_3(t, \tilde{u}, \tilde{v}, \tilde{w}) \right) + \frac{2\tilde{\alpha}}{(2-\tilde{\alpha})N(\tilde{\alpha})} \int_0^t \left(\Lambda_3(s, \tilde{u}(s), \tilde{v}(s), \tilde{w}(s)) \right) ds.\end{aligned}$$

To establish uniqueness, we analyze the difference between two functions $\tilde{u}, \tilde{u}', \tilde{v}, \tilde{v}'$, and \tilde{w}, \tilde{w}' :

$$\left\| \Lambda_1(t, \tilde{u}, \tilde{v}, \tilde{w}) - \Lambda_1(t, \tilde{u}', \tilde{v}', \tilde{w}') \right\| \leq H_1 \left\| \tilde{u} - \tilde{u}' \right\| + H_2 \left\| \tilde{v} - \tilde{v}' \right\| + H_3 \left\| \tilde{w} - \tilde{w}' \right\|,$$

where H_1, H_2 , and H_3 are constants derived using the Cauchy-Schwarz inequality and are given by:

$$\begin{aligned}H_1 &= |d_1| + |d_2| \sup |\tilde{v}|, \\ H_2 &= |d_2| \sup |\tilde{u}| + 2|d_3| \sup |\tilde{v}| + 3|d_4| \sup |\tilde{v}|^2, \\ H_3 &= |d_5| + 2|d_6| \sup |\tilde{w}| + 3|d_7| \sup |\tilde{w}|^2.\end{aligned}$$

If $H = \max(H_1, H_2, H_3)$ satisfies $H < 1$, the Banach fixed-point theorem ensures a unique solution exists. This proves that the system admits a unique solution in the considered function space.

5. Stability Analysis of Iterative Method

We use an iterative formula using the Sumudu transform [31–33] to analyze the stability of the fractional-order system (1). Using the Sumudu transform, we obtain:

$$\begin{aligned}\text{ST} \left[{}^{\text{CF}} \mathcal{D}_{0,t}^{\tilde{\alpha}} \tilde{u} \right] (s) &= \text{ST} \left[-d_1 \tilde{u} + d_2 \tilde{u}\tilde{v} + d_3 \tilde{v}^2 + d_4 \tilde{v}^3 + d_5 \tilde{w} + d_6 \tilde{w}^2 + d_7 \tilde{w}^3 + d_{20} \right] (s), \\ \text{ST} \left[{}^{\text{CF}} \mathcal{D}_{0,t}^{\tilde{\alpha}} \tilde{v} \right] (s) &= \text{ST} \left[-d_8 \tilde{u}\tilde{v} - d_9 \tilde{u}^2 - d_{10} \tilde{u}^3 + d_{11} \tilde{v}(1 - \tilde{v}) - d_{12} \tilde{w} - d_{13} \tilde{w}^2 - d_{14} \tilde{w}^3 + d_{21} \right] (s), \\ \text{ST} \left[{}^{\text{CF}} \mathcal{D}_{0,t}^{\tilde{\alpha}} \tilde{w} \right] (s) &= \text{ST} \left[d_{15} \tilde{v} + d_{16} \tilde{v}^2 + d_{17} \tilde{v}^3 - d_{18} \tilde{w} - d_{19} \tilde{v}\tilde{w} \right] (s).\end{aligned}$$

According to the Sumudu transform for the Caputo-Fabrizio derivative, the system is:

$$\begin{aligned} \frac{N(\check{\alpha})}{1 - \check{\alpha} + \check{\alpha}s} (\mathbf{ST}[\check{u}](s) - \check{u}(0)) &= \mathbf{ST} \left[-d_1 \check{u} + d_2 \check{u}\check{v} + d_3 \check{v}^2 + d_4 \check{v}^3 + d_5 \check{w} + d_6 \check{w}^2 + d_7 \check{w}^3 + d_{20} \right] (s), \\ \frac{N(\check{\alpha})}{1 - \check{\alpha} + \check{\alpha}s} (\mathbf{ST}[\check{v}](s) - \check{v}(0)) &= \mathbf{ST} \left[-d_8 \check{u}\check{v} - d_9 \check{u}^2 - d_{10} \check{u}^3 + d_{11} \check{v}(1 - \check{v}) - d_{12} \check{w} - d_{13} \check{w}^2 - d_{14} \check{w}^3 \right. \\ &\quad \left. + d_{21} \right] (s), \\ \frac{N(\check{\alpha})}{1 - \check{\alpha} + \check{\alpha}s} (\mathbf{ST}[\check{w}](s) - \check{w}(0)) &= \mathbf{ST} \left[d_{15} \check{v} + d_{16} \check{v}^2 + d_{17} \check{v}^3 - d_{18} \check{w} - d_{19} \check{v}\check{w} \right] (s). \end{aligned}$$

By rewriting these equations, we get:

$$\begin{aligned} \mathbf{ST}[\check{u}](s) &= \check{u}(0) + \frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_1 \check{u} + d_2 \check{u}\check{v} + d_3 \check{v}^2 + d_4 \check{v}^3 + d_5 \check{w} + d_6 \check{w}^2 + d_7 \check{w}^3 + d_{20} \right] (s), \\ \mathbf{ST}[\check{v}](s) &= \check{v}(0) + \frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_8 \check{u}\check{v} - d_9 \check{u}^2 - d_{10} \check{u}^3 + d_{11} \check{v}(1 - \check{v}) - d_{12} \check{w} - d_{13} \check{w}^2 - d_{14} \check{w}^3 \right. \\ &\quad \left. + d_{21} \right] (s), \\ \mathbf{ST}[\check{w}](s) &= \check{w}(0) + \frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[d_{15} \check{v} + d_{16} \check{v}^2 + d_{17} \check{v}^3 - d_{18} \check{w} - d_{19} \check{v}\check{w} \right] (s). \end{aligned}$$

The iterative scheme is obtained using the inverse Sumudu transform:

$$\begin{aligned} \check{u}_{n+1} &= \check{u}_n(0) + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_1 \check{u} + d_2 \check{u}\check{v} + d_3 \check{v}^2 + d_4 \check{v}^3 + d_5 \check{w} + d_6 \check{w}^2 \right. \right. \\ &\quad \left. \left. + d_7 \check{w}^3 + d_{20} \right] (s), \right. \\ \check{v}_{n+1} &= \check{v}_n(0) + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_8 \check{u}\check{v} - d_9 \check{u}^2 - d_{10} \check{u}^3 + d_{11} \check{v}(1 - \check{v}) - d_{12} \check{w} \right. \right. \\ &\quad \left. \left. - d_{13} \check{w}^2 - d_{14} \check{w}^3 + d_{21} \right] (s), \right. \\ \check{w}_{n+1} &= \check{w}_n(0) + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[d_{15} \check{v} + d_{16} \check{v}^2 + d_{17} \check{v}^3 - d_{18} \check{w} - d_{19} \check{v}\check{w} \right] (s). \right. \end{aligned}$$

Assuming $n \rightarrow \infty$, the approximate solutions are:

$$\check{u} = \lim_{n \rightarrow \infty} \check{u}_n, \quad \check{v} = \lim_{n \rightarrow \infty} \check{v}_n, \quad \check{w} = \lim_{n \rightarrow \infty} \check{w}_n.$$

In order to ensure convergence of the iterative method under suitable conditions, the self-mapping operator and contraction properties are examined.

Our next step is to analyze the stability of fractional CF-systems by means of these notions and relationships.

Theorem 1. Assume Ψ is a self-map:

$$\Psi(\check{u}_i) = \check{u}_{j+1} = \check{u}_i + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_1 \check{u}_i + d_2 \check{u}_i \check{v}_i + d_3 \check{v}_i^2 + d_4 \check{v}_i^3 + d_5 \check{w}_i + d_6 \check{w}_i^2 \right. \right.$$

$$\begin{aligned}
 & + d_7 \check{w}_i^3 + d_{20}](s) \Big], \\
 \Psi(\check{v}_i) &= \check{v}_{n+1} = \check{v}_i + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_8 \check{u}_i \check{v}_i - d_9 \check{u}_i^2 - d_{10} \check{u}_i^3 + d_{11} \check{v}_i(1 - \check{v}_i) - d_{12} \check{w}_i \right. \right. \\
 & \quad \left. \left. - d_{13} \check{w}_i^2 - d_{14} \check{w}_i^3 + d_{21} \right] (s) \right], \\
 \Psi(\check{w}_i) &= \check{w}_{n+1} = \check{w}_i + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[d_{15} \check{v}_i + d_{16} \check{v}_i^2 + d_{17} \check{v}_i^3 - d_{18} \check{w}_i - d_{19} \check{v}_i \check{w}_i \right] (s) \right],
 \end{aligned}$$

Then the iterative fractional CF-system is Ψ -stable in $\mathcal{L}^1(a, b)$ whenever we have:

$$\begin{cases}
 1 - d_1 + d_5 + d_2 K_2^* \Phi_1 + d_2 K_1^* \Phi_2 + 2 d_3 K_2^* \Phi_3 + 3 d_4 (K_2^*)^2 \Phi_4 + 2 d_6 K_3^* \Phi_5 + 3 d_7 (K_3^*)^2 \Phi_6 < 1, \\
 1 + d_{11} - d_8 K_2^* \Phi_7 - 2 d_9 K_1^* \Phi_8 - 3 d_{10} (K_1^*)^2 \Phi_9 - 2 d_{11} K_2^* \Phi_{10} - d_{12} \Phi_{11} - 2 d_{13} K_3^* \Phi_{12} \\
 - 3 d_{14} (K_3^*)^2 \Phi_{13} < 1, \\
 1 + d_{15} - d_{18} + 2 d_{16} K_2^* \Phi_{14} + 3 d_{17} (K_2^*)^2 \Phi_{15} + d_{19} K_3^* \Phi_{16} - d_{19} K_2^* \Phi_{17} < 1,
 \end{cases}$$

where the functions Φ_ℓ are introduced later for $k = 1, 2, \dots, 17$.

Proof. We will prove that Ψ has a fixed point. We write: $i, j \in \mathbb{N}$,

$$\begin{aligned}
 \|\Psi(\check{u}_i) - \Psi(\check{u}_j)\| &= \|\check{u}_{i+1} - \check{u}_{j+1}\| = \|\check{u}_i + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_1 \check{u}_i + d_2 \check{u}_i \check{v}_i + d_3 \check{v}_i^2 \right. \right. \\
 & \quad \left. \left. + d_4 \check{v}_i^3 + d_5 \check{w}_i + d_6 \check{w}_i^2 + d_7 \check{w}_i^3 + d_{20} \right] (s) \right] \\
 & \quad - \check{u}_j - \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_1 \check{u}_j + d_2 \check{u}_j \check{v}_j + d_3 \check{v}_j^2 \right. \right. \\
 & \quad \left. \left. + d_4 \check{v}_j^3 + d_5 \check{w}_j + d_6 \check{w}_j^2 + d_7 \check{w}_j^3 + d_{20} \right] (s) \right] \Big\| \\
 & \leq \|\check{u}_i - \check{u}_j\| + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[d_1 \|\check{u}_i - \check{u}_j\| \right. \right. \\
 & \quad + d_2 \|\check{v}_j\| \|\check{u}_i - \check{u}_j\| + d_2 \|\check{u}_i\| \|\check{v}_i - \check{v}_j\| + d_3 \|\check{v}_i + \check{v}_j\| \|\check{v}_i - \check{v}_j\| \\
 & \quad + d_4 \|\check{t}_{2,i}^2 + \check{v}_i \check{v}_j + \check{t}_{2,j}^2\| \|\check{v}_i - \check{v}_j\| + d_5 \|\check{w}_i - \check{w}_j\| + d_6 \|\check{w}_i + \check{w}_j\| \|\check{w}_i - \check{w}_j\| \\
 & \quad \left. \left. + d_7 \|\check{t}_{3,i}^2 + \check{w}_i \check{w}_j + \check{t}_{3,j}^2\| \|\check{w}_i - \check{w}_j\| \right] (s) \right].
 \end{aligned}$$

We shall consider all four solutions due to their similar roles

$$\|\check{u}_i - \check{u}_j\| \simeq \|\check{v}_i - \check{v}_j\| \simeq \|\check{w}_i - \check{w}_j\|.$$

Since the sequences $\check{u}_i, \check{v}_i, \check{w}_i$ are convergent, they are also bounded. Thus, there exist constants K_1^*, K_2^*, K_3^* such that for any t and all $i, j \in \mathbb{N}$, we have:

$$\|\check{u}_i\| \leq K_1^*, \quad \|\check{v}_j\| \leq K_2^*, \quad \|\check{w}_i\| \leq K_3^*.$$

Therefore, we obtain:

$$\|\Psi(\check{u}_i) - \Psi(\check{u}_j)\| \leq \|\check{u}_i - \check{u}_j\| + \mathbf{ST}^{-1} \left[\frac{1 - \check{\alpha} + \check{\alpha}s}{N(\check{\alpha})} \mathbf{ST} \left[-d_1 \|\check{u}_i - \check{u}_j\| \right. \right.$$

$$\begin{aligned}
& + d_2 K_2^* \|\check{u}_i - \check{u}_j\| + d_2 K_1^* \|\check{v}_i - \check{v}_j\| + 2 d_3 K_2^* \|\check{v}_i - \check{v}_j\| + 3 d_4 (K_2^*)^2 \|\check{v}_i - \check{v}_j\| \\
& + d_5 \|\check{w}_i - \check{w}_j\| + 2 d_6 K_3^* \|\check{w}_i - \check{w}_j\| + 3 d_7 (K_3^*)^2 \|\check{w}_i - \check{w}_j\| \Big] (s) \Big] \\
& = \left(1 - d_1 + d_5 + d_2 K_2^* \Phi_1 + d_2 K_1^* \Phi_2 + 2 d_3 K_2^* \Phi_3 + 3 d_4 (K_2^*)^2 \Phi_4 \right. \\
& \left. + 2 d_6 K_3^* \Phi_5 + 3 d_7 (K_3^*)^2 \Phi_6 \right) \|\check{u}_i - \check{u}_j\|.
\end{aligned}$$

Similarly, we obtain:

$$\begin{aligned}
\|\Psi(\check{v}_i) - \Psi(\check{v}_j)\| & \leq \left(1 - d_{11} - d_8 K_2^* \Phi_7 - 2 d_9 K_1^* \Phi_8 - 3 d_{10} (K_1^*)^2 \Phi_9 + 2 d_{11} K_2^* \Phi_{10} \right. \\
& \left. - d_{12} \Phi_{11} - 2 d_{13} K_3^* \Phi_{12} - 3 d_{14} (K_3^*)^2 \Phi_{13} \right) \|\check{v}_i - \check{v}_j\|,
\end{aligned}$$

and

$$\begin{aligned}
\|\Psi(\check{w}_i) - \Psi(\check{w}_j)\| & \leq \left(1 + d_{15} - d_{18} + 2 d_{16} K_2^* \Phi_{14} + 3 d_{17} (K_2^*)^2 \Phi_{15} + d_{19} K_3^* \Phi_{16} \right. \\
& \left. - d_{19} K_2^* \Phi_{17} \right) \|\check{w}_i - \check{w}_j\|.
\end{aligned}$$

Under the conditions of the theorem, Ψ is a contraction and thus has a fixed point. Applying Theorem 1, we conclude that Ψ is Pi-card Ψ -stable, completing the proof.

6. Hyers-Ulam Stability Analysis

Definition 4. Consider the fractional-order system given in (1). The system is said to satisfy Hyers-Ulam (HU) stability if there exists a positive constant C_Ψ such that for every $\varepsilon > 0$, any function $\Phi^* \in \Phi$ fulfilling the inequality:

$$\left\| {}_0^{\text{CF}} \mathcal{D}_{0,t}^{\alpha} \Phi^* - \Psi(t, \Phi^*) \right\| \leq \varepsilon, \quad \forall t \in \mathcal{J}, \quad (3)$$

admits a unique solution $\Phi \in \Phi$ to the unperturbed system satisfying the initial condition $\Phi(0) = \Phi^*(0)$, and the bound:

$$\left\| \Phi^* - \Phi \right\| \leq C_\Psi \varepsilon, \quad \forall t \in \mathcal{J}.$$

Here,

$$\Phi^* := \begin{bmatrix} y_1^* \\ y_2^* \\ y_3^* \end{bmatrix}, \quad \Phi^*(0) := \begin{bmatrix} y_1^*(0) \\ y_2^*(0) \\ y_3^*(0) \end{bmatrix}, \quad \text{and } \Psi(t, \Phi^*) := \begin{bmatrix} \Lambda_1(t, \check{u}, \check{v}, \check{w}) \\ \Lambda_2(t, \check{u}, \check{v}, \check{w}) \\ \Lambda_3(t, \check{u}, \check{v}, \check{w}) \end{bmatrix}.$$

Definition 5. The system (1) possesses generalized HU stability if there exists a function $\Gamma_\Psi : \mathcal{J} \rightarrow \mathbb{R}_+$, continuous with $\Gamma_\Psi(0) = 0$, such that for all $\Phi^* \in \Phi$ satisfying (3), there exists a unique solution $\Phi \in \Phi$ to (1) such that:

$$\left\| \Phi^* - \Phi \right\| \leq \Gamma_\Psi(\varepsilon), \quad \forall t \in \mathcal{J}.$$

Remark 1. A perturbation function $\Delta \in C(\mathcal{J})$ is introduced with the properties $\Delta(0) = 0$ and:

(i) $|\Delta| \leq \varepsilon$ for all $t \in \mathcal{J}$ and $\varepsilon > 0$;

(ii) ${}^{\text{CF}}_0 \mathcal{D}_{0,t}^{\check{\alpha}} \Phi^* = \Psi(t, \Phi^*) + \Delta$, where $\Delta = [\Delta_1, \Delta_2, \Delta_3]^T$.

Lemma 1. The perturbed solution Φ_{Δ}^* to the equation:

$$\begin{cases} {}^{\text{CF}}_0 \mathcal{D}_{0,t}^{\check{\alpha}} \Phi^* = \Psi(t, \Phi^*) + \Delta, & t \in \mathcal{J}, \\ \Phi^*(0) = \Phi_0^*, \end{cases}$$

satisfies:

$$|\Phi_{\Delta}^* - \Phi^*| \leq \Lambda \varepsilon,$$

where $\Lambda = \left[\frac{2(1-\check{\alpha})}{(2-\check{\alpha})N(\check{\alpha})} + \frac{T^{2\check{\alpha}}}{(2-\check{\alpha})N(\check{\alpha})} \right]$.

Proof. The function Φ^* satisfies:

$$\Phi^* = \Phi_0^* + \frac{2(1-\check{\alpha})}{(2-\check{\alpha})N(\check{\alpha})} \Psi(t, \Phi^*) + \frac{2\check{\alpha}}{(2-\check{\alpha})N(\check{\alpha})} \int_0^t (t-s)^{\check{\alpha}-1} \Psi(s, \Phi^*(s)) ds.$$

Utilizing the perturbation properties in Remark 1, we obtain:

$$|\Phi_{\Delta}^* - \Phi^*| \leq \Lambda \varepsilon.$$

Theorem 2. The fractional-order system (1) exhibits Hyers-Ulam (HU) stability.

Proof. Let Φ^* be an approximate solution satisfying

$$\|{}^{\text{CF}}_0 D_t^{\check{\alpha}} \Phi^*(t) - \Psi(t, \Phi^*(t))\| \leq \varepsilon, \quad \forall t \in J,$$

and let Φ be the exact solution of the system with the same initial condition.

Then, using the integral form of the Caputo-Fabrizio operator, we get

$$\begin{aligned} \|\Phi^* - \Phi\| &\leq \Lambda \varepsilon + \frac{2(1-\check{\alpha})}{(2-\check{\alpha})N(\check{\alpha})} \sup_{t \in J} \|\Psi(t, \Phi^*) - \Psi(t, \Phi)\| \\ &\quad + \frac{2\check{\alpha}}{(2-\check{\alpha})N(\check{\alpha})} \sup_{t \in J} \int_0^t (t-s)^{\check{\alpha}-1} \|\Psi(s, \Phi^*(s)) - \Psi(s, \Phi(s))\| ds. \end{aligned}$$

Assuming that Ψ satisfies a Lipschitz condition with constant L_{Ψ} , we obtain:

$$\|\Phi^* - \Phi\| \leq \Lambda \varepsilon + \left[\frac{2(1-\check{\alpha})}{(2-\check{\alpha})N(\check{\alpha})} + \frac{T^{\check{\alpha}}}{(2-\check{\alpha})N(\check{\alpha})} \right] L_{\Psi} \|\Phi^* - \Phi\|.$$

Rearranging gives:

$$\|\Phi^* - \Phi\| \leq \frac{2\Lambda}{1 - \Lambda L_{\Psi}} \varepsilon,$$

provided that $\Lambda L_{\Psi} < 1$. Thus, the system is Hyers-Ulam stable.

7. Parameter Sensitivity Indices

A key aspect of evaluating our model’s robustness is sensitivity analysis, which examines how variations in parameters influence system stability and glucose regulation. We assess the impact of small perturbations in critical parameters such as: Insulin absorption rate ($\check{\alpha}$), Glucose utilization rate (γ), Delay effects ($\check{\alpha}$), Fractional order ($\check{\alpha}$). The following table presents the sensitivity indices for each parameter with respect to the state variables: insulin (\check{u}), glucose (\check{v}), and beta-cell mass (\check{w}). The sensitivity indices presented in Table 2 were computed using the following formula:

$$S_{d_j}^{t_i} = \frac{\partial t_i}{\partial d_j} \times \frac{d_j}{t_i},$$

where:

- t_i is the steady-state or selected state value of the variable \check{u} , \check{v} , or \check{w} .
- $\frac{\partial t_i}{\partial d_j}$ is the partial derivative of t_i with respect to the parameter d_j .

These derivatives were computed numerically using finite difference approximations by perturbing each parameter slightly (for example, by 1%) and observing the corresponding change in the output variables. The relative effect of each parameter on the state variables was then quantified using the sensitivity formula. From Table 2, we observe the following

Parameter	Value	Interpretation
d ₁	2.04	Baseline insulin degradation rate in the absence of glucose.
d ₂	0.10	Insulin secretion rate modulated by glucose presence.
d ₃	1.09	Glucose-dependent enhancement of insulin production.
d ₄	-1.08	Autonomous insulin secretion rate from $\check{\alpha}$ -cells.
d ₅	0.03	Minor contribution of $\check{\alpha}$ -cells to insulin levels.
d ₆	-0.06	Reduction in insulin due to secondary regulatory effects.
d ₇	2.01	Positive feedback of $\check{\alpha}$ -cells on insulin release.
d ₈	0.22	Insulin’s influence on glucose utilization.
d ₉	-3.84	Glucose reduction rate driven by insulin secretion.
d ₁₀	-1.20	Secondary glucose depletion due to insulin action.
d ₁₁	0.30	Natural glucose production rate in the absence of insulin.
d ₁₂	1.37	Suppression of glucose due to insulin from $\check{\alpha}$ -cells.
d ₁₃	-0.30	Negative contribution of $\check{\alpha}$ -cell insulin to glucose reduction.
d ₁₄	0.22	Modulation of glucose levels through $\check{\alpha}$ -cell insulin activity.
d ₁₅	0.30	Glucose-induced stimulation of $\check{\alpha}$ -cell activity.
d ₁₆	-1.35	Suppressive effect of glucose on $\check{\alpha}$ -cell dynamics.
d ₁₇	0.50	Positive regulation of $\check{\alpha}$ -cell function by glucose.
d ₁₈	-0.42	Inhibitory feedback of glucose on $\check{\alpha}$ -cells.
d ₁₉	-0.15	Secondary glucose-driven downregulation of $\check{\alpha}$ -cells.
d ₂₀	-0.19	Constant flux term in glucose homeostasis.
d ₂₁	-0.56	Basal insulin production rate under normal conditions.

Table 1: Parameter descriptions based on Shabestari et al. [66].

key insights:

- The parameters d₁₈ and d₁₉, which control the decrease of beta-cell mass, have the most significant impact on \check{w} , with large negative sensitivity values.

Parameter	$S_{\check{u}}$	$S_{\check{v}}$	$S_{\check{w}}$
d ₁	-1.4584	0.3645	-0.3076
d ₂	5.7196	-2.0144	1.3324
d ₃	13.8271	-6.4371	2.8303
d ₄	20.1587	-9.1741	4.2190
d ₅	0.7411	-0.5713	-0.0556
d ₆	0.0172	0.3869	-0.0042
d ₇	-0.6560	1.2357	0.0236
d ₈	-2.3575	0.8510	-0.6028
d ₉	0.4925	-0.3288	0.0561
d ₁₀	0.9667	-0.7072	0.1009
d ₁₁	-2.5487	0.5221	-0.7848
d ₁₂	-2.4446	2.0981	-0.1940
d ₁₃	-1.3511	1.3557	-0.0446
d ₁₄	-0.4730	0.7695	0.0795
d ₁₅	-37.0338	10.5529	-10.0360
d ₁₆	-36.4639	6.4340	-11.2552
d ₁₇	-37.0735	2.3980	-12.8421
d ₁₈	-224.8819	19.8675	-78.3221
d ₁₉	-222.4813	22.9688	-76.4388
d ₂₀	1.5168	-1.6664	-0.1389
d ₂₁	3.8009	-3.0403	0.3757

Table 2: Sensitivity indices of the parameters in the glucose-insulin-beta cell model.

- The parameters d_{15}, d_{16}, d_{17} , related to the increase of beta-cells due to glucose, strongly influence insulin (\check{u}), showing large negative indices.
- The glucose-insulin interaction terms, represented by d_8, d_9 , and d_{10} , contribute significantly to changes in glucose levels (\check{v}).
- Some parameters, such as d_6 and d_7 , have minimal effects on all state variables.

7.1. Model Mean and Confidence Interval

In this study, parameters for the glucose-insulin system are obtained from experimental data and previous literature. The initial conditions for the state variables are set as follows: $\check{u}(0) = 100$, $\check{v}(0) = 10$, and $\check{w}(0) = 5$. The parameters used in the model are summarized in Table 1.

To estimate the expected solution of the stochastic fractional glucose-insulin model, Euler-Maruyama approximations were computed using 10,000 sample paths for discretizations $N = 2^9, 2^{10}, 2^{11}, 2^{12}, 2^{13}$ over $[0, 1]$.

Tables 3 and 4 present the mean and 95% confidence intervals for \check{u} , \check{v} , and \check{w} over time.

The mean and 95 % confidence intervals for the state variables \tilde{u} , \tilde{v} , and \tilde{w} (Tables 3 and 4) were estimated using stochastic simulation.

The procedure involved:

- Solving the stochastic version of the fractional glucose-insulin system using the Euler-Maruyama method.
- Running 10,000 independent sample paths for each time step to account for stochastic variability.
- Computing the expected (mean) values at each discrete time point using:

$$E[X] \approx \frac{1}{10000} \sum_{i=1}^{10000} X_N^i,$$

where X_N^i is the value of the i -th sample path at the final time $T = 1$ for a given number of subintervals N .

- Constructing the 95% confidence intervals by extracting the 2.5th and 97.5th percentiles from the empirical distribution of the simulated values.

t_i	\bar{t}_1	95% Confidence Interval		\bar{t}_2	95% Confidence Interval	
		Lower bound	Upper bound		Lower bound	Upper bound
0	100	95	105	10	8	12
0.1	98	94	102	9.5	7.5	11.5
0.2	96	92	100	9	7	11
0.3	94	90	98	8.5	6.5	10.5
0.4	92	88	96	8	6	10
0.5	90	86	94	7.5	5.5	9.5
1	80	76	84	6	4	8

Table 3: Mean and 95% confidence intervals for \tilde{u} (Glucose concentration) and \tilde{v} (Insulin concentration).

t_i	\bar{t}_3	95% Confidence Interval	
		Lower bound	Upper bound
0	5	4	6
0.1	5.2	4.2	6.2
0.2	5.4	4.4	6.4
0.3	5.6	4.6	6.6
0.4	5.8	4.8	6.8
0.5	6	5	7
1	7	6	8

Table 4: Mean and 95% confidence intervals for \tilde{w} (Regulatory factor).

8. Numerical Methods

8.1. Generalized Caputo-Fabrizio Operator and Discrete Scheme

Definition 6. The Sobolev space $W_2^1(0, m)$ is defined as the set of functions $h(t)$ on the interval $(0, m)$ such that:

- $h(t) \in L^2(0, m)$, i.e., the function is square integrable on $(0, m)$,
- and its weak derivative $h'(t) \in L^2(0, m)$.

Formally, we write:

$$W_2^1(0, m) = \left\{ h(t) \in L^2(0, m) \mid \frac{dh(t)}{dt} \in L^2(0, m) \right\}.$$

Let $\{t_\ell\}_{\ell=0}^n$ be a uniform partition of the interval $[0, m]$ with step size $\Delta t = t_{\ell+1} - t_\ell$. Let $h_\ell = h(t_\ell)$ denote the numerical approximation of the function $h(t)$ at the discrete time point t_ℓ . Here, $\alpha_\ell \in [t_\ell, t_{\ell+1}]$ is a point within the integration interval, as guaranteed by the mean value theorem for integrals, at which the second derivative of $g(\xi, h(\xi))$ is evaluated.

The CF operator introduces a contemporary modification to fractional calculus by using a kernel free from singularities. For a function $h(t) \in W_2^1(0, m)$ and a parameter $\check{\alpha} \in [0, 1]$, it is defined as:

$${}_0^{\text{CF}} \mathcal{D}_t^{\check{\alpha}} h(t) = \frac{N(\check{\alpha})}{1 - \check{\alpha}} \int_0^t \frac{d}{d\xi} h(\xi) \exp \left[-\frac{\check{\alpha}}{1 - \check{\alpha}} (x - \xi) \right] d\xi,$$

where $N(\check{\alpha})$ is a normalizing function with properties $N(0) = 1$ and $N(1) = 1$. The related fractional integral with an exponential kernel is expressed as:

$${}_0^{\text{CF}} I_x^{\check{\alpha}} (h(t)) = \frac{1 - \check{\alpha}}{N(\check{\alpha})} h(t) + \frac{\check{\alpha}}{N(\check{\alpha})} \int_0^t h(\xi) d\xi.$$

Now, let us consider the Cauchy-type problem for this operator:

$${}_0^{\text{CF}} \mathcal{D}_t^{\check{\alpha}} h(t) = g(t, h(t)),$$

which, when recast in integral form, becomes:

$$h(t) - h(0) = \frac{1 - \check{\alpha}}{N(\check{\alpha})} g(t, h(t)) + \frac{\check{\alpha}}{N(\check{\alpha})} \int_0^t g(\xi, h(\xi)) d\xi.$$

At discrete points, we write:

$$h(t_{\ell+1}) - h(0) = \frac{1 - \check{\alpha}}{N(\check{\alpha})} g(t_\ell, h(t_\ell)) + \frac{\check{\alpha}}{N(\check{\alpha})} \int_0^{t_{\ell+1}} g(\xi, h(\xi)) d\xi,$$

and similarly for t_ℓ :

$$h(t_\ell) - h(0) = \frac{1 - \check{\alpha}}{N(\check{\alpha})} g(t_{\ell-1}, h(t_{\ell-1})) + \frac{\check{\alpha}}{N(\check{\alpha})} \int_0^{t_\ell} g(\xi, h(\xi)) d\xi.$$

Subtracting the two, we get:

$$h(t_{\ell+1}) - h(t_\ell) = \frac{1 - \check{\alpha}}{N(\check{\alpha})} \left[g(t_\ell, h(t_\ell)) - g(t_{\ell-1}, h(t_{\ell-1})) \right] + \frac{\check{\alpha}}{N(\check{\alpha})} \int_{t_\ell}^{t_{\ell+1}} g(\xi, h(\xi)) d\xi.$$

By applying Lagrange interpolation, we approximate:

$$\begin{aligned} h(t_{\ell+1}) - h(t_\ell) &= \frac{1 - \check{\alpha}}{N(\check{\alpha})} \left[g(t_\ell, h(t_\ell)) - g(t_{\ell-1}, h(t_{\ell-1})) \right] \\ &+ \frac{\check{\alpha}}{N(\check{\alpha})} \int_{t_\ell}^{t_{\ell+1}} \left(\frac{g(t_\ell, h(t_\ell))}{\Delta t} (\xi - t_{\ell-1}) - \frac{g(t_{\ell-1}, h(t_{\ell-1}))}{\Delta t} (\xi - t_\ell) \right) d\xi. \end{aligned}$$

The resulting numerical method becomes:

$$h(t_{\ell+1}) = h(t_\ell) + \frac{1 - \check{\alpha}}{N(\check{\alpha})} \left[g(t_\ell, h(t_\ell)) - g(t_{\ell-1}, h(t_{\ell-1})) \right] + \frac{\check{\alpha}}{N(\check{\alpha})} \left(g(t_\ell, h(t_\ell)) \frac{3}{2} \Delta t - g(t_{\ell-1}, h(t_{\ell-1})) \frac{1}{2} \Delta t \right).$$

8.2. Error Estimation

To assess the efficiency of this numerical scheme, consider the Cauchy problem:

$$\begin{cases} {}_0^{\text{CF}} \mathcal{D}_t^{\check{\alpha}} h(t) = g(t, h(t)), \\ h(0) = h_0. \end{cases}$$

Assuming that $g(t, h(t))$ has a bounded second derivative, the error term $F_\ell^{\check{\alpha}}$ can be written as:

$$F_\ell^{\check{\alpha}} = \frac{\check{\alpha}}{N(\check{\alpha})} \int_{t_\ell}^{t_{\ell+1}} \frac{(\xi - t_\ell)(\xi - t_{\ell-1})}{2!} \frac{\partial^2}{\partial \xi^2} [g(\xi, h(\xi))]_{\xi=\check{\alpha}_\ell} d\xi.$$

Taking the supremum of the second derivative provides the error bound:

$$\left| F_\ell^{\check{\alpha}} \right| \leq \frac{\check{\alpha}}{N(\check{\alpha})} \sup_{\xi \in [0, t_{\ell+1}]} \left| \frac{\partial^2}{\partial \xi^2} g(\xi, h(\xi)) \right| \frac{5}{12} (\Delta t)^3.$$

8.3. Numerical Illustrations

Systems (1) and (2) are numerically solved using the proposed fractional Caputo-Fabrizio scheme, with initial conditions $\check{u}(0) = 0$, $\check{v}(0) = 1.5$, and $\check{w}(0) = 1$. The parameter values are adopted from Shabestari et al. [66].

Figures 1, 3, and 5 (a)–(c) display the time series of the uncontrolled CF fractional system (1), while Figures 2, 4, and 6 (a)–(c) show the corresponding controlled CF fractional system (2), for the following cases:

$$\rho = 0.98, \quad \rho = 0.97 + 0.03 \times \tanh\left(\frac{t}{10}\right), \quad \text{and} \quad \rho = 0.97 + 0.03 \times \sin\left(\frac{t}{10}\right).$$

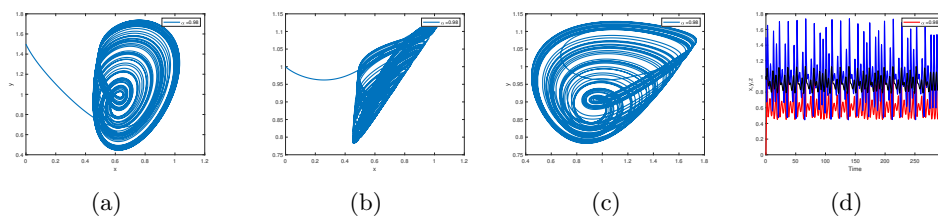


Figure 1: Synchronization of system (1), illustrated in (a)-(d) for $\tilde{\alpha} = 0.98$.

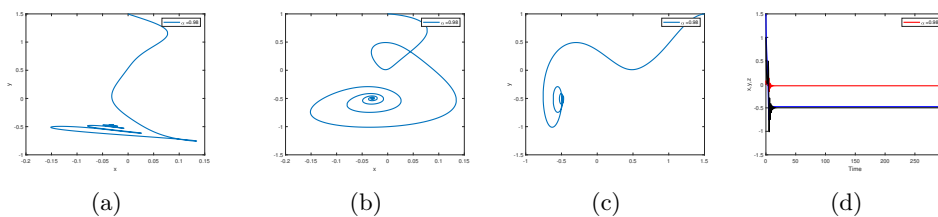


Figure 2: System synchronization (2), illustrated in (a)-(d) for $\tilde{\alpha} = 0.98$.

9. Discussion

Based on our fractional-order glucose-insulin model, memory effects play a significant role in diabetes management. According to sensitivity analysis, the order of the fractional derivative strongly impacts the model’s behavior, emphasizing the importance of fractional calculus. Our approach aligns more effectively with real-world patient data than conventional integer-order models.

Contrary to classical models, our model captures long-term glucose and insulin variations. Because of this capability, individualized insulin therapy strategies can be developed. Using the Sumudu transform, we enable real-time simulations for clinical applications.

Certain limitations warrant further investigation. Fractional-order models improve accuracy, but parameter estimation remains challenging. Real-world validation through clinical trials is crucial to verify the model’s applicability across diverse populations. The use of machine learning techniques in real-time applications will enhance parameter estimation and improve predictive accuracy.

An extensive sensitivity analysis was conducted to assess the robustness of our fractional-order glucose-insulin model. Specifically, we examined the influence of fractional-order parameters $\tilde{\alpha}$, insulin absorption rates, and glucose utilization rates on system stability. Fractional derivatives are suitable for capturing memory-dependent processes since small variations in $\tilde{\alpha}$ significantly affect glucose-insulin interactions. The most critical factors in determining steady-state glucose levels are insulin degradation and glucose uptake, according to sensitivity indices.

To validate our results, we compared them with existing integer-order and fractional-order models. Our fractional-order approach provides superior predictive accuracy and reproduces observed glucose fluctuations more accurately than classical models. Addi-

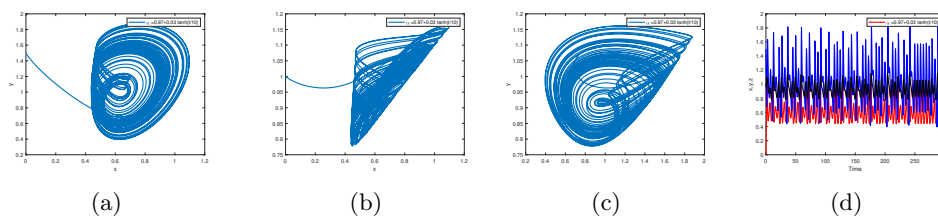


Figure 3: Synchronization of system (1), illustrated in (a)-(d) for $\check{\alpha} = 0.97 + 0.03 \times \tanh(t/10)$.

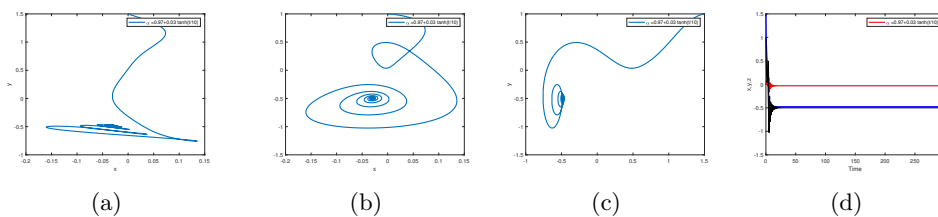


Figure 4: System synchronization (2), illustrated in (a)-(d) for $\check{\alpha} = 0.97 + 0.03 \times \tanh(t/10)$.

tionally, our computational methodology enhances numerical stability in integer-order formulations to minimize oscillatory behavior. The Sumudu transform also facilitates more efficient solution derivation than standard numerical solvers.

Our study has significant implications for diabetes management. Due to our model’s improved accuracy and stability, it can be integrated into personalized treatment plans, allowing precise insulin dosing based on individual metabolic responses. A linear control strategy can also optimize insulin pump algorithms, reducing the risk of severe glucose fluctuations and improving patient outcomes. A model that accounts for fractional-order dynamics in glucose regulation can be used to predict disease progression and refine therapeutic interventions, ultimately leading to more effective and adaptive diabetes management. Fractional calculus advances diabetes care by providing more realistic and flexible models. These findings contribute to improved glucose regulation strategies that improve diabetes patients’ quality of life.

In Table 5, we demonstrate how this study differs from previous research. This study introduces a novel fractional-order glucose-insulin model formulated in the Caputo-Fabrizio sense, capturing the non-local memory effects inherent in glucose metabolism. By leveraging the Sumudu transform for analytical solution construction and employing Hyers-Ulam stability analysis, we establish both robustness and reliability of the model under perturbations. Moreover, the development of a linear control strategy and the exploration of synchronization phenomena under variable-order fractional dynamics mark significant advancements in the mathematical modeling of diabetes. These contributions provide a new theoretical foundation for personalized insulin therapy and real-time blood glucose regulation.

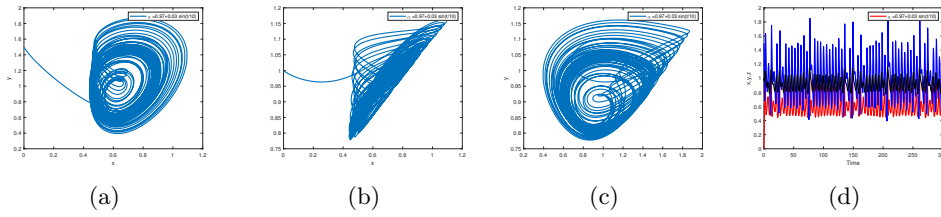


Figure 5: Synchronization of system (1), illustrated in (a)-(d) for $\tilde{\alpha} = 0.97 + 0.03 \times \sin(t/10)$.

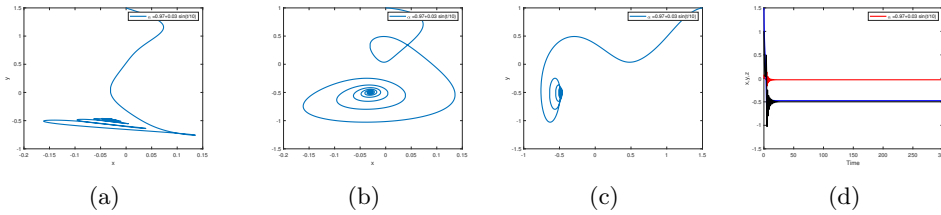


Figure 6: System synchronization (2), illustrated in (a)-(d) for $\tilde{\alpha} = 0.97 + 0.03 \times \sin(t/10)$.

Aspect	Previous Studies	Our Study
Mathematical Framework	Integer-order ODEs	Fractional Caputo-Fabrizio derivatives
Solution Approach	Standard solvers	Sumudu Transform-based infinite series solutions
Stability Analysis	Not considered or minimal	Hyers-Ulam stability rigorously examined
Control Mechanism	Limited or absent	Linear control strategy introduced
Clinical Relevance	Generic models with limited adaptability	Personalized treatment insights for diabetes management

Table 5: Comparison of Our Study with Previous Research

10. Conclusion

In this study, we explored the chaotic behavior of a variable-order glucose-insulin regulatory system using fractional differential operators with an exponential decay kernel.

Our findings demonstrate that fractional operators significantly influence the system's chaotic dynamics, with exponential decay kernels introducing long-range memory effects that lead to increased complexity and unpredictability, while localized dynamics under other conditions exhibit faster convergence to equilibrium. Using fixed-point theory, we established the uniqueness and boundedness of solutions, and due to the model's high nonlinearity, a numerical scheme was employed. Through variable-order numerical methods, we effectively captured the chaotic nature of glucose-insulin interactions, showing improved accuracy over traditional approaches. This enhanced understanding of memory effects and chaos contributes to the development of more effective strategies for diabetes control and offers a promising foundation for optimizing insulin delivery systems. Building on these findings, future research can focus on generalizing the model to include physiological factors such as glucagon dynamics, physical activity, stress, and circadian rhythms; incorporating stochastic modeling to reflect real-world variability; calibrating the model using continuous glucose monitoring and insulin pump data; designing advanced adaptive control algorithms for artificial pancreas systems; integrating machine learning for prediction and decision support; and validating the model through clinical trials to ensure its reliability and applicability in personalized diabetes management.

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